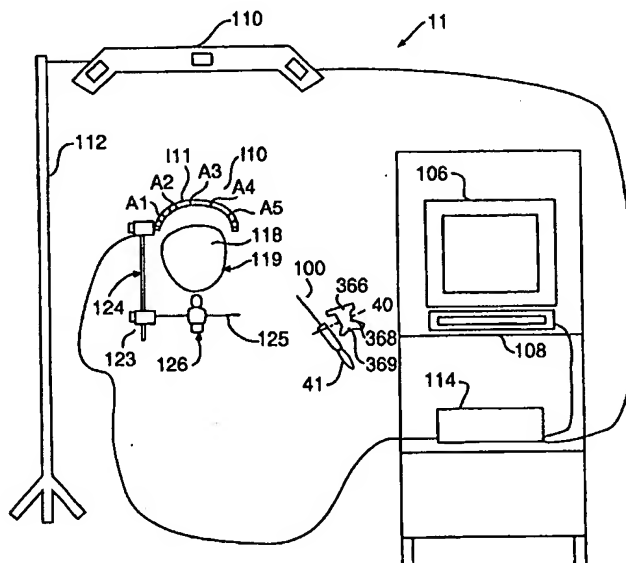




INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶ : A61B 19/00	A1	(11) International Publication Number: WO 99/33406 (43) International Publication Date: 8 July 1999 (08.07.99)
<p>(21) International Application Number: PCT/US98/27841</p> <p>(22) International Filing Date: 30 December 1998 (30.12.98)</p> <p>(30) Priority Data: 09/001,956 31 December 1997 (31.12.97) US</p> <p>(71) Applicant: SURGICAL NAVIGATION TECHNOLOGIES, INC. [US/US]; 530 Compton Street, Broomfield, CO 80020 (US).</p> <p>(72) Inventors: HUNTER, Mark, W.; 204 Summit Trail, Broomfield, CO 80020 (US). KESSMAN, Paul, J.; 2190 W. 10th Avenue #203, Broomfield, CO 80020 (US). SMITH, Scott, R.; P.O. Box 219, Marine, IL 62061 (US).</p> <p>(74) Agents: COLAIANNI, Jennifer, M. et al.; Finnegan, Henderson, Farabow, Garrett & Dunner, L.L.P., 1300 I Street, N.W., Washington, DC 20005-3315 (US).</p>	<p>(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, UZ, VN, YU, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).</p> <p>Published <i>With international search report.</i></p>	

(54) Title: **WIRELESS PROBE SYSTEM FOR USE WITH A STEREOTACTIC SURGICAL DEVICE**

(57) Abstract

A trackable wireless probe for use in a computer assisted image guided medical and surgical navigation systems that provides wireless localization to images during medical and surgical procedures. The probe has emitters for being tracked by the system. The probe includes a control circuit for activating the emitters in a predetermined pattern recognizable by the system. The system includes a reference arc positioned relative to the patient which also includes emitters. The emitters on the reference arc activated and tracked during times that the emitters on the probe are inactive.

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	.YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakhstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

WIRELESS PROBE SYSTEM FOR USE WITH A STEREOTACTIC SURGICAL DEVICE

Description

BACKGROUND OF THE INVENTION

Technical Field

The present invention relates generally to computer assisted image guided medical and surgical navigation systems that generate images during medical and surgical procedures indicating the relative position of various body parts, surgical implants, and instruments. In particular, the present invention relates to a system of determining the position of a wireless reference probe or arc using a sequenced lighting pattern to synchronize lights on the probe and reference arc or frame to determine a position of each.

Background Art

Computer assisted image guided medical and surgical navigation systems are known and used to generate images in order to guide a doctor during a surgical procedure. Such systems are disclosed, for example, in U.S. Patent No. 5,383,454 to Bucholz; PCT Application No. PCT/US94/04530 (Publication No. WO 94/24933) to Bucholz; and PCT Application No. PCT/US95/12984 (Publication No. WO 96/11624) to Bucholz et al., incorporated herein by reference.

In general, these image guided systems use images of a body part, such as CT scans, taken before surgery to generate images on a display, such as a CRT monitor screen, during surgery for representing the position of a surgical instrument with respect to the body part. The systems typically include tracking devices such as, for example, an LED array mounted on a surgical instrument as well as a body part, a digitizer or a camera device to track in real time the position of the LED arrays and thus the body part and the instrument used during surgery, and a monitor screen to display images

representing the body part and the position of the instrument relative to the body part as the surgical procedure is performed.

Current stereotactic surgical systems such as that described in the United States Patent 5,383,454 and PCT Application No. PCT/US95/12984, disclose a system tracking a probe as well as a body part during surgery. As described therein, a reference arc or frame is positioned in fixed relation to the head of a patient. Both the probe and the reference arc include emitters which are detected and used by a processing system to determine the position of the probe and arc in three dimensional space. In these prior art systems, both the reference arc and the probe must receive external signals, typically through a wire or cable or other suitable connection, for activating the emitters. The surgeon typically initiates these external signals by, for example, depressing a button on a foot switch. The button may be connected to a processor that sends a signal to the probe emitters directing them to emit radiation. The processor must also direct the emitters on the reference arc to light. One problem with this prior art system is that the wires that connect the probe to the processor can interfere with the surgeon's work. In addition, the surgeon must take the time to press the foot pedal; otherwise, he may not receive constant updates on the probe position without repeatedly hitting the floor pedal.

Disclosure of the Invention

Systems and methods consistent with the present invention include a device to determine a position of a probe with respect to an object, such as, for example, a cranium or spinal vertebrae. A reference arc has a first set of emitters positioned on it and is fixedly positioned on the object. A probe has a second set of emitters positioned on it and is positioned by a surgeon near the object. An activating circuit in the probe causes each of the second set of emitters to turn on and off in a predetermined sequence to produce a first ordered pattern of light. A detector which is part of a digitizer, is positioned to detect radiation from the first and second set of emitters. A processor includes instructions for recognizing the ordered pattern output by the second set of emitters based on the radiation detected by the detector and for

instructing the first set of emitters to turn on and off in a second ordered pattern that limits overlap with the first ordered pattern, whereby a position of both the reference arc and the probe may be determined by the processor based on detected radiation.

In an alternate embodiment the reference arc includes an activating circuit for lighting the first set of emitters in a pattern.

In an alternate embodiment the probe includes an activating circuit that lights emitters on the probe at a different rate than an activating circuit in the reference arc lights emitters on the arc. A processor includes instructions for recognizing the differing ordered pattern outputs of the set of emitters on the arc and probe, whereby a position of both the reference arc and the probe may be determined based on detected radiation.

A method is also provided for indicating a position of a surgical instrument comprising the steps of positioning a reference arc near a patient and emitting radiation using a first set of emitters positioned on the reference arc. Radiation is emitted from a second set of emitters positioned on a second structure in an ordered pattern. Detectors detect radiation from the first and second set of emitters. The ordered pattern is recognized by a processor based on detected radiation. The processor activates the first set of emitters during times when the second set of emitters is inactive, whereby a position of the reference arc and surgical instrument may be determined based on detected radiation.

It is to be understood that both the foregoing general description and the following detailed description are exemplary and explanatory and are not restrictive of the invention as claimed.

Brief Description of the Drawings

The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate embodiments of the invention and, together with the description, serve to explain the objects, advantages and principles of the invention. In the drawings,

Fig. 1 is a schematic front view of a computer assisted image guided surgery system used with a wireless probe according to the present invention;

Fig. 2 shows a control circuit that is positioned in the probe shown in Fig. 1 according to the present invention;

Fig. 3 shows a timing diagram of the pattern of activation of the LEDs on the probe using the control circuit of Fig. 2 and includes the timing of activation of the LEDs on a reference arc activated by the system shown in Fig. 2 and the detection frames and localization frames of the processor;

Fig. 4 shows a flow chart of the steps for initializing the system of the present invention and determining the position of the probe and reference arc;

Fig. 5 shows a timing diagram of the emission of light from the reference arc and the probe according to one embodiment of the present invention; and

Fig. 6 shows a timing diagram of the emission of light from the reference arc and the probe according to one embodiment of the present invention.

Best Mode for Carrying Out the Invention

Reference will now be made in detail to the present preferred embodiments of the invention, examples of which are illustrated in the accompanying drawings. Wherever possible, the same reference numbers are used in the drawings and the description to refer to the same or like parts.

The medical instrument of the present invention is shown generally as part of the system 11 in Fig. 1. An instrument such as probe 100 can be used in known computer assisted image guided surgical navigation systems such as the system 11 shown in Fig. 1 and disclosed in PCT Application No. PCT/US95/12984 (Publication No. WO 96/11624) to Bucholz et al. A computer assisted image guided surgery system 11 generates an image for display on a CRT monitor 106 representing the real time position of a body part such as a cranium, represented generally by circle 119, having reference points 118 and the position of probe 100 relative to the body part 119.

An image may be generated on monitor 106 from an image data set stored in a controller, such as computer 108, usually generated preoperatively

by some scanning technique such as, for example, by a CT scanner or by magnetic resonance imaging (MRI). The image data set and the image generated have reference points for at least one body part. The reference points for the particular body part have a fixed spatial relation to the particular body part.

System 11 also generally includes a processor for processing image data, shown as computer 108, and displays this processed data on monitor 106. Digitizer control unit 114 is under control of computer 108. Digitizer 114, in conjunction with a reference frame or arc 120 and a sensor array 110 or other known position sensing unit, tracks the real time position of a body part, such as a cranium shown at 119 clamped in reference arc 120, and a probe 100. Reference arc 120 has emitters 122 (such as LEDs A1, A2, A3, A4, and A5) or other tracking means that generate signals representing the position of the various body reference points. Reference arc 120 is fixed spatially in relation to a body part by a clamp assembly indicated generally at 124, 125, and 126, so that arc 120 moves as the body part is moved during surgery. Probe 100 also has a tracking device shown as an emitter array set 40 (such as LEDs 366, 368, 369) which generates signals representing the position of the probe during the procedure.

Sensor array 110, mounted on support 112, receives and in conjunction with digitizer 114 and computer 108, triangulates the signals generated by emitters 122 and emitter array set 40 in order to identify during the procedure the relative position of the reference points on arc 120 and the probe 100. Digitizer 114 and computer 108 may then modify the image data set according to the identified relative position of each of the reference points during the procedure. Computer 108 may then generate an image data set for display on monitor 106 representing the position of the body part and the probe on the appropriate CT or MRI scan slice during the operation. The general structure and operation of an image guided surgery system is well known in the art and need not be discussed further here.

In order to initiate the emitters on a reference arc and probe some prior art systems required the surgeon to take a positive action such as pressing a

foot switch connected to a digitizer 114 attached by a cable to a probe 100. However, this unduly burdened the surgeon and might not provide for continual and easy updates on the position of the probe. The present invention does not require any action on the part of the surgeon to activate emitters on the reference arc and eliminates the need for the surgeon to attach a cable to the probe 100 to activate the emitters.

Fig. 1 shows the probe 100 having a body 41 and an emitter set 40. Probe 100 may be any one of a plurality of types of surgical instruments such as a surgical coagulating forceps, a bipolar coagulating forceps, drill, suction tube, bayonet cauterizing device, catheter guide, drill guide, or any other surgical instrument modified as discussed with respect to Figs. 2-4. Probe 100 can be wireless and has a battery 361 for power and internal circuitry shown in Fig. 2 for controlling the light emitter set 40. In one embodiment a switch may be on the probe to activate and disable the emitter set 40.

The probe 100 includes within body 41 a control circuit 362 for controlling the emission of light from emitter set 40. Figure 2 shows the control circuit 362 hardware that includes a microprocessor 364 shown as the Motorola 68HC705J2CS. Any suitable microprocessor or pattern generator circuit known in the art may be used. Control circuit 362 drives the light emitter set 40 which includes at least two light emitters, but as shown includes three LEDs 366, 368, and 369, all suitably positioned on the probe 100 for monitoring by sensor array 110. PA0 output 18 drives the first LED 366, PA1 output 17 drives the second LED 368, and PA2 output 16 drives the third LED 369. If additional emitters are desired, then other outputs such as 11-15 may act as drivers. The clock timer signal generated by the 4 megahertz crystal of clock 370 is input to OSC1 and OSC2.

Further with respect to Fig. 2, the microprocessor 364 includes routine software and hardware for controlling the emitters on the probe 100 to generate signals to drive the emitter set 40. The present invention activates the emitters on the probe 100 in a predetermined ordered pattern such as that indicated generally at 400 in Fig. 3. The probe of the present invention behaves independently of the digitizer 114 in that probe 100 is not connected

or controlled by the digitizer 114. The probe 100 includes the internal circuitry described above for activating the emitters on the probe 100 in a predetermined order at predetermined times. This order and timing of activating the emitters is referred to as an ordered pattern. One example of the pattern is illustrated in Fig. 3. Other patterns in addition to that of Fig. 3, such as any cyclical pattern with a sufficient period for detection by digitizer 114, may also be used as long as both the digitizer 114 and/or the computer 108 are programmed so the digitizer 114 can recognize the same predetermined pattern produced by probe 100. The computer 108 has a memory which is programmed beforehand to store the predefined pattern 400 and this pattern 400 can be programmed into the digitizer 114 during initialization; therefore the digitizer 114 can recognize the pattern 400 when output by the probe 100.

Preferably the emission of radiation from one LED does not overlap with that of another LED. There may be empty time between emitter transitions. Preferably there is an empty time cycle between transitioning from the probe to the arc to account for errors in the synchronization. In addition in a preferred embodiment the geometry of the emitters based on detected radiation may be determined to verify that the detected structure is the appropriate shape for the probe or arc. This best fit geometry check can be performed to verify correct synchronization throughout the localization process.

The timing diagram of Fig. 3 is divided into time slots, with each time slot generally corresponding to a LED activation period shown as 1-20 on the bottom of the drawing. All the time slots do not necessarily have to be equal; but in a preferred embodiment, each time slot is about 30 milliseconds.

With reference to Fig. 3, control circuit 362 activates (turns on lights) first emitter LED 366 for the first time slot S1 of the pattern 400. Then control circuit 362 activates LED 368 for the second time slot S2. Next, a third LED 369 is activated for a third time slot S3. The emitters are on for the entire time slot and preferably the emitters are activated sequentially such that the end of the first time slot corresponds to the start of the second time slot.

Preferably the periods of activation do not overlap and there may be time gaps between the periods of activation. Changes to these parameters merely change the pattern 400. A correspondingly similar pattern 400 must be stored in both probe 100 and also the computer 108 to enable the digitizer 114 to recognize the pattern.

After the sequential lighting of the LED set 40, the clock 370 input to microprocessor 364 counts seven time slots (slots S4-S10) represented as T1-T7 in Fig. 3 during which the probe 100 does not activate any of the emitters. Microprocessor 364 does not directly control emitters 122 on the reference arc 120; instead, in this embodiment, the computer 108 controls emitter set 122, which includes emitters A1-A5. The timing diagram shows the emission of radiation from emitters A1-A5, which can begin - as described in further detail below - after the probe pattern is recognized and synchronization has occurred. The overall pattern 400 generated by the probe 100 alone includes sequencing through ten equal time slots - three of which include a single LED being lit and the other seven of which include no action. During the period of no action by the probe, the computer 108 will activate emitters A1-A5 on the reference arc 120. Once the probe completes its pattern 400, the pattern 400 is restarted at the beginning with LED 366 by the microprocessor.

Referring to Fig. 4, a flow chart is provided further showing the steps of the present invention. The microprocessor 364 of probe 100 activates LEDs 366, 368, and 369 and executes the pattern 400 in Fig. 3 (step 500) independently of any other parts of the system shown in Fig. 1. While the pattern 400 is being executed, the sensor array 110 detects light output by LEDs 366, 368, and 369 on the probe 100. During this initializing period, the emitter set 122 on the reference arc 120 are not activated by the computer 108. The probe 100 executes the pattern of emission 400 for LEDs 366, 368, and 369 as shown in Fig. 3. Sensor array 110 is constantly detecting received light (step 510).

After a suitable initialization period, the digitizer 114 samples the received light in units called detection frames to recognize the probe's 100

pattern 400. As illustrated in Fig. 3, detection frames 115 are each at a fraction of the probe's 100 emitter activation time (oversampling), that is the time each emitter is on, so that the digitizer 100 can determine when the probe 100 emitters are on and off. The detection frames sampling rate must be at least two times the individual emitter rate (nyquist criteria), but it is preferable to use a faster sampling rate such as four times the emitter lighting rate. The more samples that are taken in a given time period the greater the precision of determining when the emitters are on or off. In this example of Fig. 3, it can be seen that for this example there are about four frames per time slot. Based on knowing detection frames where light is detected and times that no light is detected above a threshold, the digitizer 114 recognizes the pattern 400 (step 520).

The digitizer 114 has an internal clock timer that preferably runs at the same frequency (or integral multiples thereof) as the clock timer 370 of the probe. Based on the recognized pattern 400, the digitizer 114 synchronizes the pulse rate of the emitters 122 on the reference arc 120 to that of the emitters 40 on the probe 100 (step 530). Synchronization of signals is well known in the art and need not be discussed further. Once pulse rates are synchronized, the digitizer 114 knows the times at which the light emitter set 40 on the probe 100 will light and defines localization frames 116 for the times at which the LEDs on the probe light (step 540). The digitizer 114 can then direct the emitters 122 on the reference arc 120 to sequentially light, A1-A5, at times when the LEDs on the probe are not lit (step 550). The digitizer 114 samples the sensor array 110 at times when emitters are expected to be on shown as probe localization frames 116 and can also sample for arc localization frames 117 (step 560). The position of the reference arc 120 and the probe 100 may now be calculated as is known in the art (step 570).

If the probe signal is lost for a significant time, such as for example when the surgeon may remove the probe from the digitizer 114 lines of sight, the digitizer 114 will assume the probe is off. The digitizer 114 will then attempt to resynchronize using detection frames until the pattern 400 of the probe 100 is recognized. The probe signal could be lost if it were blocked or

the clock signal were out of phase. Once resynchronized, the digitizer 114 resumes processing as discussed above.

In another embodiment of the present invention, the circuit shown in Fig. 2 can be included in the reference arc 120 instead of the probe 100 so that the reference arc can be wireless and independently perform the pattern 400 of Fig. 3. In this case, computer 108 does not activate the emitters on the reference arc but must synchronize and recognize the reference pattern 400 in the same manner discussed above with respect to the probe. In this embodiment, it is the probe instead of the arc that may be wired and controlled by the digitizer 114.

In yet another embodiment of the present invention, the circuit shown in Fig. 1 can be included in both the probe 100 and reference arc 120. Therefore, both devices can be wireless and independently perform different patterns that can be recognized by the digitizer 114. In this case one of the device will have a pattern that is half the period of the other or differing patterns that can be recognized. The digitizer 114 will distinguish between lights on the arc and the probe by using a known geometry of the probe and the arc to determine which detected lights belong to which element. The pattern and detection of the same are repeated allowing for enough data points of lights to be detected to determine a geometry of the detected lights. Once synchronized, the digitizer 114, as discussed for the previous embodiment, can know the times at which lights are to be expected to be lit from both the probe and the arc. Figs. 5 and 6 show example timing diagrams corresponding to this embodiment. As shown in Figs. 5 and 6 the probe is localized during periods where only the probe emitters 366, 368, and 369 are on and the reference arc 120 is localized during periods when only the emitters A1-A5 on the reference arc are on. Fig. 5 shows an example where the patterns of both the emitters on the reference arc 120 and the probe 100 are close in phase and Fig. 6 show an example where the patterns of both the emitters on the reference arc 120 and the probe 100 are out of phase. During periods when both the emitters on the probe and on the arc are off, the digitizer 114 may turn on emitters on a third device, such as

another probe to detect the position of the third device. For example, in Fig. 6 during the no localization period when both the emitters on the probe and arc are off, the digitizer 114 may initiate LEDs to light on a third structure.

The pattern lighting registration system of the present invention may be used in connection with any type of image guided surgery system including those described in U.S. Patent No. 5,383,454 to Bucholz; PCT Application No. PCT/US94/04530 (Publication No. WO 94/24933) to Bucholz; and PCT Application No. PCT/US95/12984 (Publication No. WO 96/11624) to Bucholz et al.

In another embodiment, the emitters on either the probe or the reference arc are replaced with reflectors that reflect light emitted from an external source, such as the digitizer unit. In this case either the probe or reference arc with reflectors will be localized during the A1-A5 cycles.

Systems and methods consistent with the present invention allow for a probe or reference arc used in image guided surgery to be continuously and easily monitored without the surgeon having to repeatedly initiate the monitoring or having the surgical instruments cabled. This is achieved by placing emitters on the probe 100 or reference arc 120 that light in an ordered pattern 400 recognized by a processor so that the processing system knows the times at which the emitters will be activated.

The foregoing description is presented for purposes of illustration and description. It is not intended to be exhaustive or to limit the invention to the precise form disclosed, and modifications and variations are possible in light of the above teachings or may be acquired from practice of the invention. The embodiments were chosen and described in order to explain the principles of the invention and its practical application to enable one skilled in the art to utilize the invention in various embodiments and with various modifications as are suited to the particular use contemplated. The scope of the invention is defined by the following claims and their equivalents.

Claims

1. A system for indicating a position of an object during surgery using a device to determine a position of the object based on received radiation from said object, said system comprising:

a first set of emitters positioned on a first structure;

a second set of emitters positioned on a second structure;

an activating circuit in the second structure for causing each of the second set of emitters to turn on and off in a predetermined sequence to produce a first ordered pattern;

a detector for detecting radiation from the first and second set of emitters; and

a processor configured to:

a) recognize the ordered pattern output by the second set of emitters based on the radiation detected by the detector; and

b) instruct the first set of emitters to turn on and off in a second ordered pattern that limits overlap with the first ordered pattern, whereby a position of the first and second structure may be determined based on detected radiation.

2. The system according to claim 1 wherein said processor includes a first clock running at a first frequency and the second structure includes a second clock running at said first frequency.

3. The system according to claim 1 wherein said processor includes a first clock running at a first frequency and the second structure includes a second clock running at a multiple of said first frequency.

4. The system according to claim 2 further including means for synchronizing the second clock to the first clock based on the recognized pattern.

5. The system according to claim 1 wherein the second set of emitters comprises at least two emitters and further includes:

means for generating a pattern of radiation that includes sequentially enabling one emitter of said at least two emitters for a first period of time, enabling another emitter of said at least two emitters for a second period of time, disabling both emitters for a third period of time, and enabling first set of emitters emit radiation during said third period of time.

6. The system according to claim 5 wherein said second structure includes a second clock and said processor includes a first clock and wherein said processor is further configured to:

sample radiation readings from said detector at a sampling rate more than the first and second periods of time; and
synchronize the first clock to the second clock.

7. The system according to claim 1 further including:

reference points means in fixed relation to the body part of the patient, wherein said first structure is in fixed relation to the reference points means;

a memory storing images of the body part, said images including reference images corresponding to the reference points means;

wherein said processor is further configured to

determine the position of the second structure relative to the first structure based on radiation detected from the first and second set of emitters;

measure the position of the reference points means relative to the first structure thereby determining the position of the second structure relative to the reference points means;

translate the determined position of the second structure into a coordinate system corresponding to the images of the object; and

means for displaying an image of the body part which corresponds to the translated position of the second structure.

8. The system according to claim 1 wherein the second structure further includes:

a switch for disabling the second set of emitters.

9. A method for indicating a position of a surgical instrument comprising the steps of:

emitting radiation using a first set of emitters positioned on a first structure;

5 emitting radiation from a second set of emitters positioned on a second structure in an ordered pattern;

detecting radiation from the first and second set of emitters; and

recognizing the ordered pattern output by the second set of emitters based on the radiation detected; and

10 activating the first set of emitters during times that the second set of emitters are inactive, whereby a position of the first and second structure may be determined based on detected radiation.

10. The method according to claim 9 wherein the second set of emitters includes at least two emitters, said method further including the steps of:

5 generating a pattern of radiation that includes sequentially enabling one emitter of said at least two emitters for a first period of time, enabling a second emitter of the at least two emitters for a second period of time and disabling both emitters for a third period of time, whereby said first set of emitters radiate during the third period of time.

11. The method according to claim 9 further including the steps of:
determining the position of the second structure relative to the first
structure based on radiation detected from the first and second set of
emitters;

5 measuring the position of reference points on the body part relative to
the first structure thereby determining the position of the second structure
relative to the reference points means;

10 translating the determined position of the second structure into a
coordinate system corresponding to images of the object stored in a memory,
said images including reference images corresponding to the reference
points; and

displaying an image of the body part which corresponds to the
translated position of the second structure.

12. A probe for use with a image guiding surgical system, the probe
comprising:

a probe body;

at least two emitters positioned on said probe body; and

5 an activating circuit positioned in the probe body for causing the
emitters to radiate in an ordered pattern.

13. The probe according to claim 12 wherein the activating circuit
includes means for sequentially enabling one emitter of said at least two
emitters for a first period of time, enabling another emitter of said at least two
10 emitters for a second period of time and disabling both emitters for a third
period of time.

14. The probe according to claim 12 further including:

a battery for powering the emitters and activating circuit thereby
allowing for a wireless probe.

15. The probe according to claim 12 further including:
a switch for disabling the emitters.

16. A reference structure for use with a image guiding surgical system,
the reference structure comprising:

a body;

at least three emitters positioned on said body; and

5 an activating circuit positioned in the body for causing the emitters to
radiate in an ordered pattern.

17. The reference structure according to claim 16 wherein the
activating circuit includes means for sequentially enabling one emitter of said
at least three emitters for a first period of time, enabling another emitter of
10 said at least three emitters for a second period of time and disabling both
emitters for a third period of time.

18. The reference structure according to claim 16 further including:
a battery for powering the emitters and activating circuit thereby
allowing for a wireless reference structure.

19. The reference structure according to claim 16 further including:
a switch for disabling the emitters.

20. A system for indicating a position of an object during surgery using
a device to determine a position of the object based on received radiation
from said object, said system comprising:

a first set of emitters positioned on a first structure;

5 an activating circuit positioned in the first structure for causing each of
the first set of emitters to turn on and off in a predetermined sequence to
produce a first ordered pattern;

a second set of emitters positioned on a second structure;

an activating circuit positioned in the second structure for causing each
10 of the second set of emitters to turn on and off in a predetermined sequence
to produce a second ordered pattern, said second ordered pattern being
different than said first ordered pattern;

a detector for detecting radiation from the first and second set of
emitters; and

15 a processor configured to recognize the first and second ordered
pattern output by the first and second set of emitters based on the radiation
detected by the detector, whereby a position of the first and second structure
may be determined based on detected radiation.

21. The system according to claim 20 wherein the second ordered
pattern has a period one-half of a period of the first ordered pattern

22. A system for indicating a position of an object during surgery using
a device to determine a position of the object based on received radiation
from said object, said system comprising:

a first structure;
5 a light source;
a set of reflectors positioned on said first structure;
a second structure;
a set of emitters positioned on said second structure;
an activating circuit positioned in the second structure for causing the
10 set of emitters to output radiation in a predetermined sequence to produce a
first ordered pattern;

a detector for detecting radiation from the set of reflectors and the set
of emitters; and

a processor configured to:
15 a) recognize the ordered pattern output by the set of emitters
based on the radiation detected by the detector; and
b) instruct a light source to light the set of reflectors in a second
ordered pattern that limits overlap with the first ordered pattern, whereby a

position of the first and second structure may be determined based on
detected radiation.

23. A system for indicating a position of an object during surgery using
a device to determine a position of the object based on received radiation
from said object, said system comprising:

- a first structure;
- a set of processor controlled emitters positioned on said first structure;
- a light source;
- a second structure;
- a set of reflectors positioned on said second structure;
- a detector for detecting radiation from the set of reflectors and the set
of emitters; and
- a processor configured to:
 - a) recognize the geometric pattern based on the radiation
detected by the detector on the second structure; and
 - b) instruct the set of emitters to turn on and off in a first ordered
pattern that limits overlap with the light source detection of the second
structure, whereby a position of the first and second structure may be
determined based on detected radiation.

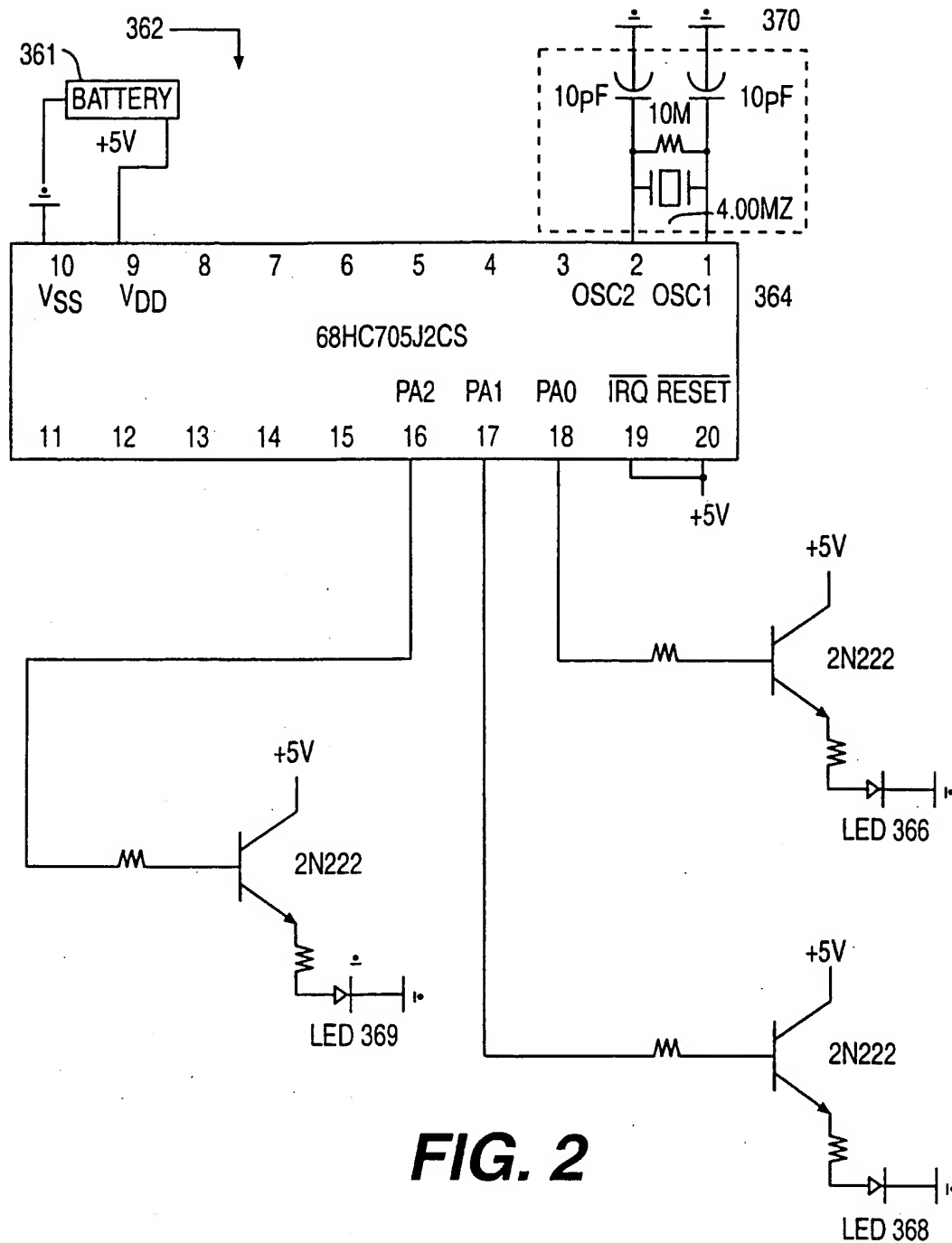
24. A system for indicating a position of an object during surgery using
a device to determine a position of the object based on received radiation
from said object, said system comprising:

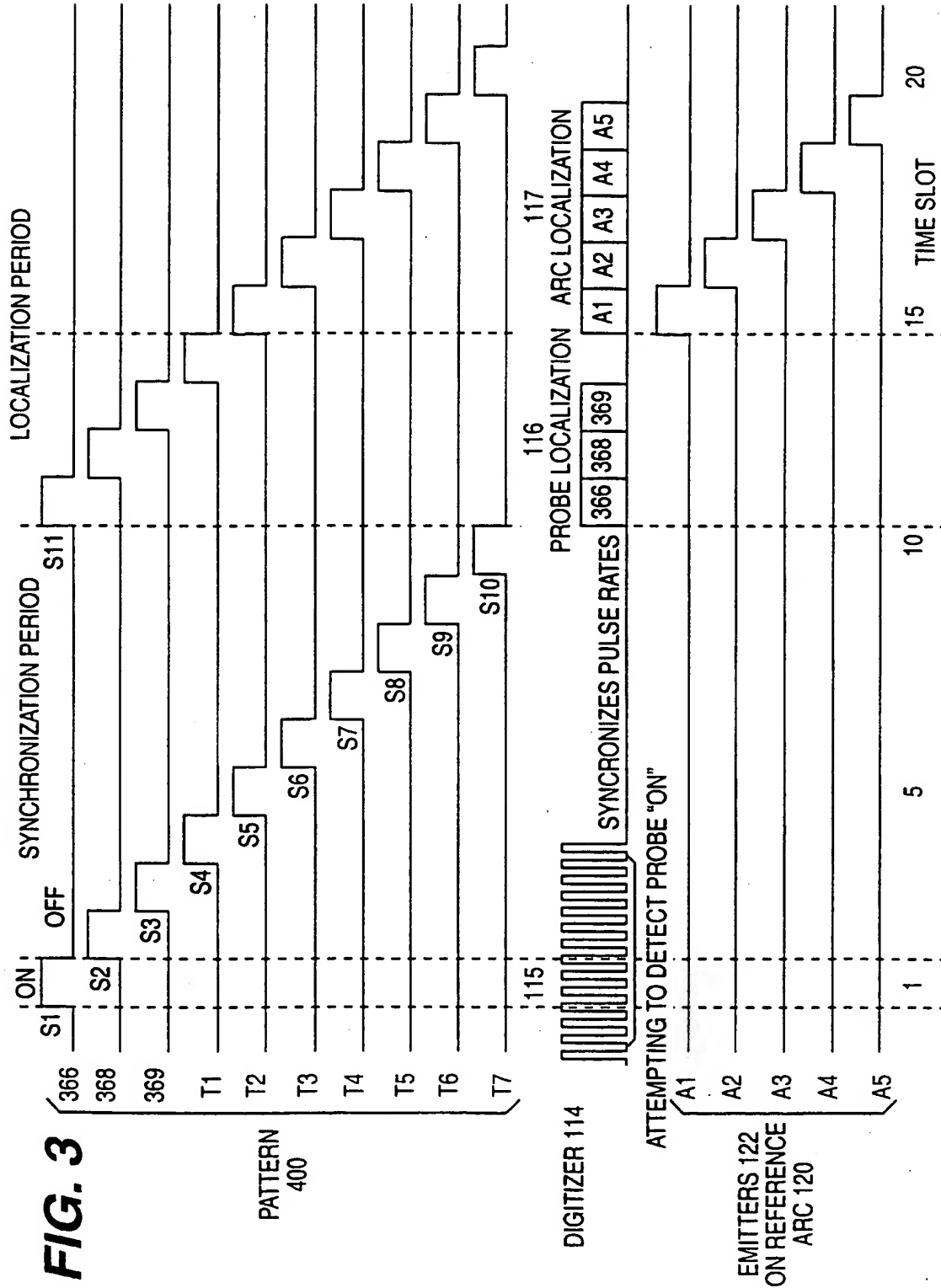
- a set of emitters positioned on an object;
- an activating circuit positioned in the object for causing each of the
emitters to turn on and off in a predetermined sequence to produce an
ordered pattern;
- a detector for detecting radiation from the set of emitters; and
- a processor configured to recognize the ordered pattern output by the
set of emitters based on the radiation detected by the detector, whereby a
position of the object may be determined based on detected radiation.

25. The system according to claim 24 wherein the object is a probe.

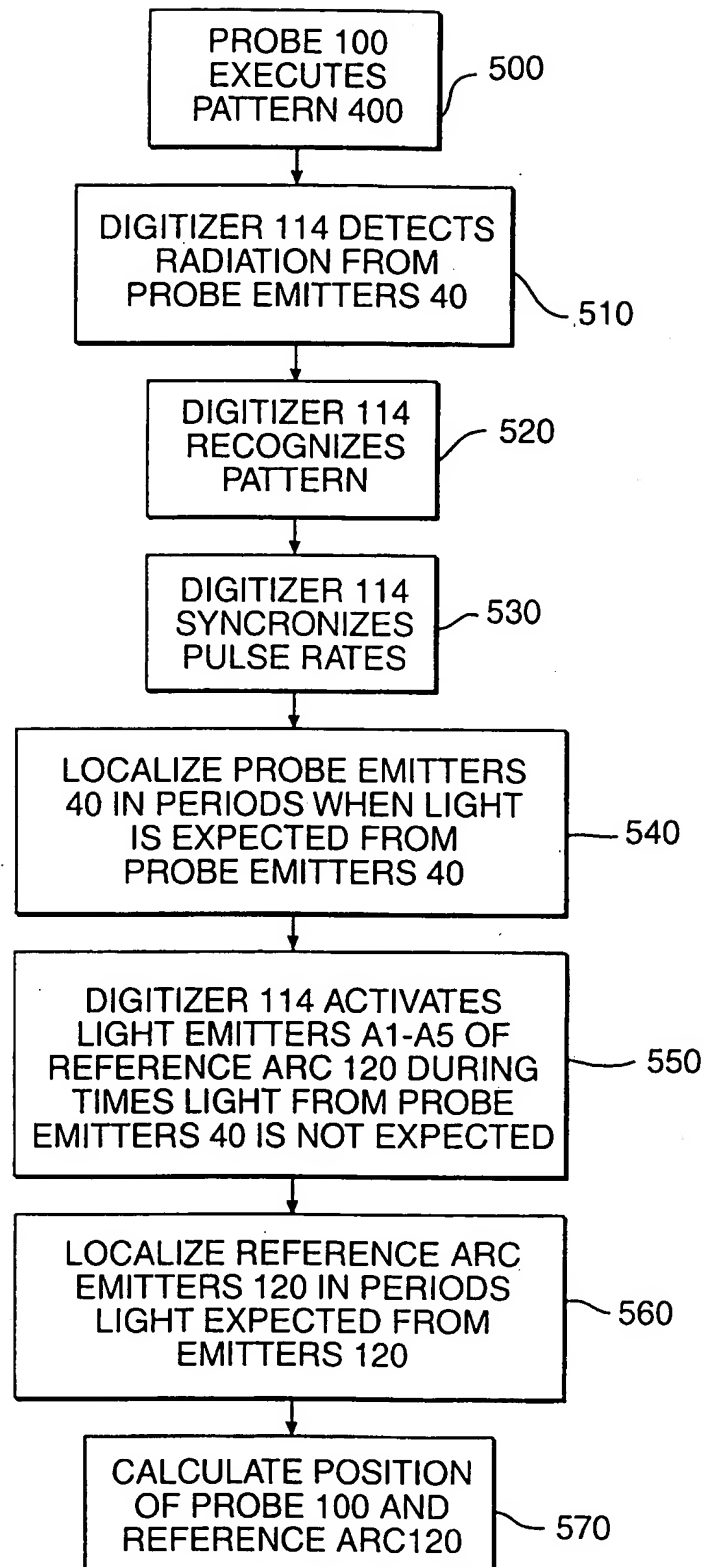
26. The system according to claim 24 wherein the object is a reference structure.

2 / 6

**FIG. 2**



4 / 6

**FIG. 4**

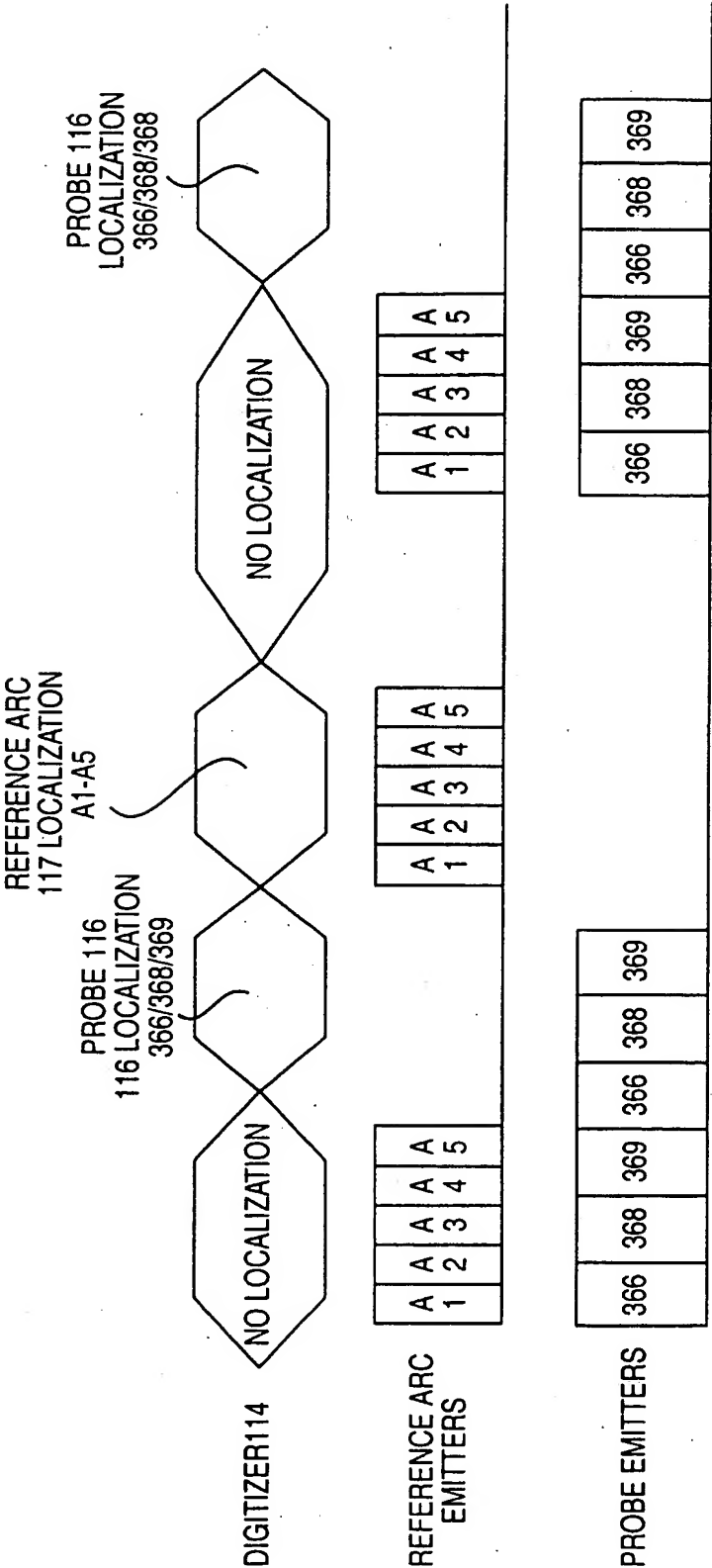


FIG. 5

6 / 6

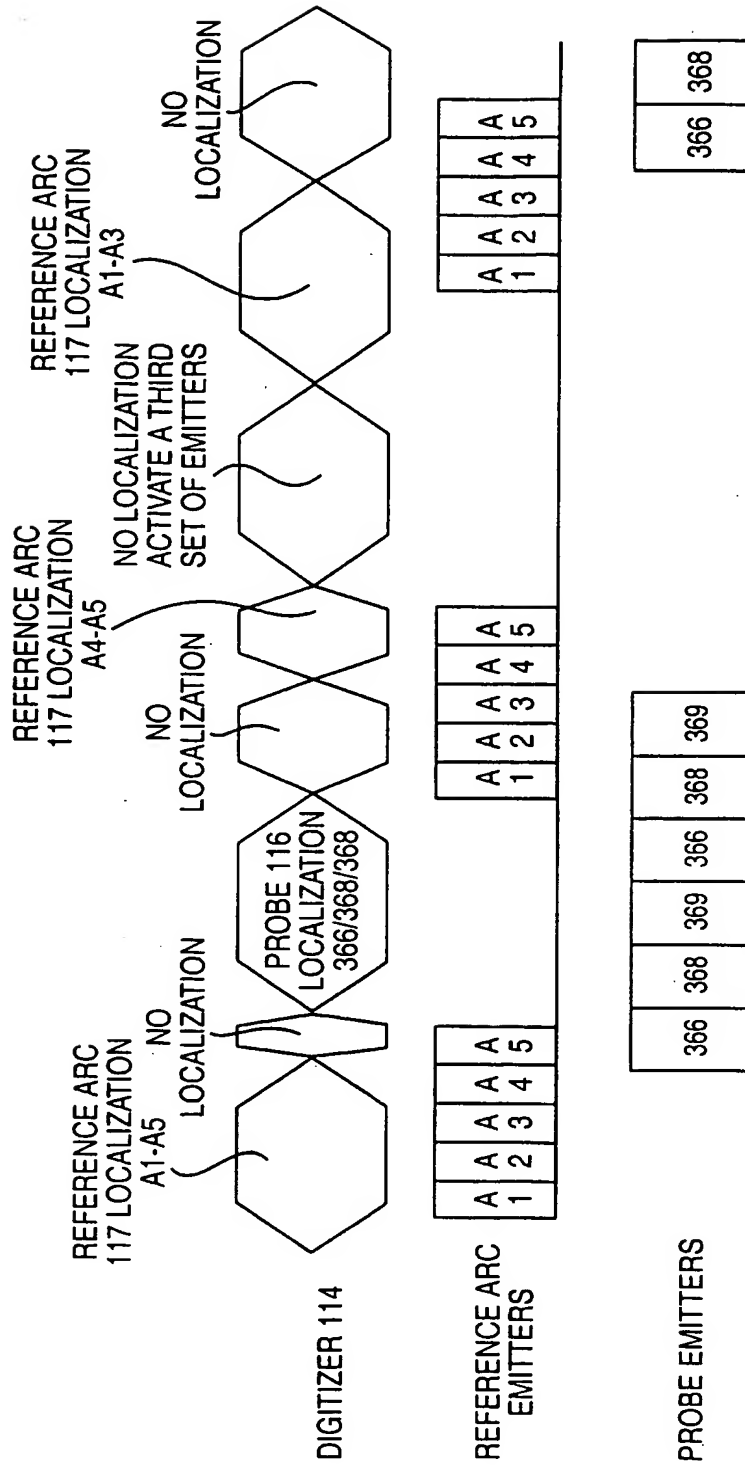


FIG. 6

INTERNATIONAL SEARCH REPORT

Int. Patent Application No.

PCT/US 98/27841

A. CLASSIFICATION OF SUBJECT MATTER

IPC 6 A61B19/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X A	WO 95 25475 A (ELEKTA INSTR AB ;HAAKANSSON HAAKAN (SE)) 28 September 1995 (in particular: 111.5 on pages 2 and 5) see the whole document	12-19, 24-26 1,7,9, 22,23
X A	US 5 622 170 A (SCHULZ WALDEAN A) 22 April 1997 see column 5, line 30 - column 6, line 9 see column 7, line 1 - column 9, line 17; claims; figures	12-19, 24-26 1,7,9,20
X A	WO 96 11624 A (BUCHOLZ RICHARD D ;BASS DANIEL (US); FOLEY KEVIN T (US); POPE TODD) 25 April 1996 cited in the application see page 29, line 15 - page 32, line 2; figures	12-19, 24-26 1,7,9,22
	-/--	

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

Date of the actual completion of the international search

5 March 1999

Date of mailing of the international search report

12/03/1999

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
Fax: (+31-70) 340-3016

Authorized officer

Manschot, J

INTERNATIONAL SEARCH REPORT

In tional Application No

PCT/US 98/27841

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	DE 42 25 112 C (BODENSEEWERK GERAETETECH) 9 December 1993 see column 2, line 40 - line 51 see column 3, line 11 - column 5, line 5; claims; figures 1,2	12-19, 24-26
A	---	1,7,9,20
A	WO 94 24933 A (UNIV ST LOUIS) 10 November 1994 cited in the application see page 16, paragraph 3 - page 19, paragraph 1; figures 4-8 -----	1,7,9, 12,16,22

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 98/27841

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
WO 9525475	A	28-09-1995	EP 0738129 A	23-10-1996
			SE 9400987 A	25-09-1995
US 5622170	A	22-04-1997	US 5383454 A	24-01-1995
			AU 6666894 A	08-11-1994
			CA 2161126 A	27-10-1994
			EP 0700269 A	13-03-1996
			IL 109385 A	10-03-1998
			JP 8509144 T	01-10-1996
			WO 9423647 A	27-10-1994
			ZA 9402812 A	22-11-1995
			AU 8876391 A	20-05-1992
			CA 2094251 A,C	20-04-1992
			DE 9117261 U	06-08-1998
			EP 0553246 A	04-08-1993
			SE 9301262 A	18-06-1993
			WO 9206645 A	30-04-1992
			US 5851183 A	22-12-1995
WO 9611624	A	25-04-1996	AU 3950595 A	06-05-1996
			CA 2201877 A	25-04-1996
			DE 29521895 U	10-09-1998
			EP 0869745 A	14-10-1998
DE 4225112	C	09-12-1993	NONE	
WO 9424933	A	10-11-1994	AU 6818694 A	21-11-1994
			CA 2161430 A	10-11-1994
			DE 9422172 U	06-08-1998
			EP 0699050 A	06-03-1996
			US 5871445 A	16-02-1999

**This Page is Inserted by IFW Indexing and Scanning
Operations and is not part of the Official Record**

BEST AVAILABLE IMAGES

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

- ☐ BLACK BORDERS
- ☐ IMAGE CUT OFF AT TOP, BOTTOM OR SIDES
- ☒ FADED TEXT OR DRAWING
- ☐ BLURRED OR ILLEGIBLE TEXT OR DRAWING
- ☐ SKEWED/SLANTED IMAGES
- ☐ COLOR OR BLACK AND WHITE PHOTOGRAPHS
- ☐ GRAY SCALE DOCUMENTS
- ☒ LINES OR MARKS ON ORIGINAL DOCUMENT
- ☐ REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY
- ☐ OTHER: _____

IMAGES ARE BEST AVAILABLE COPY.

As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.